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Phase Sensitivity of Bipolar EEG Training Protocols

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TECHNICAL NOTE

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Phase Sensitivity of Bipolar EEG Training Protocols

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ABSTRACT. *Introduction.* When performing bipolar EEG training the reward waveform is dependent on the phase relationship between the two sites at the center frequency of the reward band. It is also driven by the instantaneous amplitude at the two sites. Effectively, the training rewards an increase in differential mode activity while discouraging common mode activity. This follows from the fact that the in-phase component of the signal is suppressed in the differential amplifier, and only the out-of-phase component of the waveforms is propagated and rewarded. These relationships can be represented visually with a vector calculation.

Method. Two vectors representing the signals at the two sites at a given frequency were combined with varying phase angle and for several representative magnitudes to yield the net output amplitude. Surrogate data were used to obtain distributions illustrating the above functional relationships.

Results. Varying phase angle between the two vectors has the greatest effect on the resultant magnitude when there is a high degree of amplitude parity. The influence of phase is more modest when comodulation is low. In cases of high amplitude disparity bipolar training reduces effectively to single-site or referential training.

Discussion. The theoretical rationale behind bipolar training as a primary approach to self-regulation is modest at this time. The present modeling of signal interaction illustrates that phase relationships play a governing role in bipolar training in the general case. That dependence is modulated by the degree of comodulation between the sites. Hence, bipolar training may activate different mechanisms of control depending upon the degree of amplitude parity between the two

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sites. The incorporation of such thinking will likely lead to a further refinement of treatment protocols. doi:10.1300/J184v10n01_06

KEYWORDS. Phase, vector analysis, Monte Carlo, bipolar, interhemispheric

INTRODUCTION

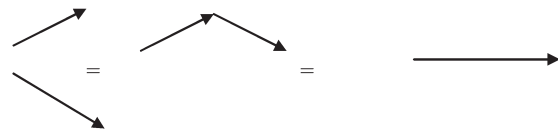
Neurofeedback with bipolar montage is finding increasing application, particularly with interhemispheric placement at homologous sites. Despite the increased utilization of this protocol, published scientific evidence as to its effectiveness remains sparse (Quirk, 1995; Sime, 2004; Putman, Othmer, Othmer, & Pollock, 2005). Clinical utilization is further inhibited by an ambiguity as to just what is being accomplished with the training. The response to reinforcement of amplitude in a narrow reward band appears to be different from conventional up-training with referential placement (Putman, 2002). Because of the growing interest in the face of this residual ambiguity, an investigation into specifically how the brain is being challenged in this protocol is warranted.

All conventional EEG biofeedback to date has been performed with EEG amplifiers with a differential first stage. This is intended to reject extraneous common-mode signals appearing at both active terminals, and has the consequence that common-mode EEG signals are rejected as well. Thus, when bipolar placement is employed clinically, only the activity which differs between the two sites is processed in the down-stream electronics. Thus in-phase, or synchronous, activity is suppressed, and out-of-phase as well as opposite-phase activity is propagated and ultimately rewarded.

As a result, the reward waveform is determined primarily by the phase relationship prevailing at the two sites at the center frequency of the reward band. It is also determined by the instantaneous amplitudes at the two sites. It is useful to examine the mathematical particulars in order to make these dependences explicit. These matters are introduced with a vector analysis, and followed with a Monte Carlo calculation of the typical response to be expected in feedback for random inputs.

VECTOR ANALYSIS

In single-channel training, the amplitude alone is at issue, a scalar quantity. When two signals are being compared, the phase difference between them is relevant, and a vector analysis is mandated. A vector, quite simply, is a directed line segment in Euclidean space that has both direction and magnitude. When a vector is rotated at a fixed rate through an angle of 2π radians (360 degrees), a sine wave is produced along each of the axes. We can essentially think of vectors as displacements. As such, in order to add two vectors, we simply need to find the single displacement that yields the same result as doing the two displacements separately. In our modeling, the “displacement” involves the magnitude of two separate signal generators. As will be shown, the magnitude of the resultant vector is determined by not only the magnitude of the two individual vectors but by the phase relationship between them. The basic approach to vector addition involves the “parallelogram law of addition” wherein the tail of one is adjoined to the point of another.



For simplicity, consider the amplitudes (A and B) of two vectors (V1 and V2) to be 100 μ V. The phase angle between the 2 vectors is ϕ (or “phi”).

In the complex plane we have:

Equation 1:

$$\begin{aligned} V1 + V2 &= A(e^{j\omega t}) + B(e^{j(\omega t + \phi)}) \\ &= A[\cos(\omega t) + j \sin(\omega t)] + B[\cos(\omega t + \phi) + j \sin(\omega t + \phi)]. \end{aligned}$$

The sinusoidal dependence is time-invariant (i.e., periodic), so it can be conveniently taken out of the discussion. That is to say, it is only the relative phase that is of interest. (This is the equivalent of talking about the angular separation between two sites on the equator without worrying about the fact that both sites are rotating about the earth's axis.) For simplicity, therefore, it is sufficient to take a snapshot at $t = 0$. This means that V_1 will be assigned a phase of zero degrees. Thus,

$$\text{with } \omega t = 0 \text{ and } A = B = 100;$$

$$\text{where } \sin(\omega t) = 0 \text{ and } \cos(\omega t) = 1$$

Equation 1 becomes:

$$100 + 100 [\cos(\phi) + j \sin(\phi)]$$

Example: for $\phi = \pi/4$ (or 45 degrees)

$$V_2 = 100 [\cos(\pi/4) + j \sin(\pi/4)]$$

$$= 70 + j70$$

$$\text{thus } V_1 + V_2 = 100 + 70 + j70$$

where the magnitude of resulting vector (V_r) = 184

$$\text{and angle of } V_r = \text{arcTan}(70/170) = \pi/8$$

(Note that the angle of V_r is not a phase angle.)

For $V_1 + V_2$ we then have the following relationship between amplitude and phase (Figure 1).

Conversely, in Figure 2 we have for $V_1 - V_2$:

Equation 2:

$$V_1 - V_2 = 100 - 100[\cos(\phi) + j \sin(\phi)];$$

$$\text{for } \phi = \pi/4$$

$$= 100 - 70 - j70 = 30 - j70$$

$$\text{which implies that } V_r = 71$$

When adding vectors, $V_1 + V_2$ yield a magnitude that is inversely related to increasing phase angle, as shown in Figure 1. The maximum amplitude is attained at $\phi = 0$ degrees and the minimum at $\phi = 180$ deg. This situation applies when rewarding a frequency in a "sum of channels" mode (with common reference), in

FIGURE 1. Relationship between amplitude and phase of the sum where V_1 and V_2 are equal in value.

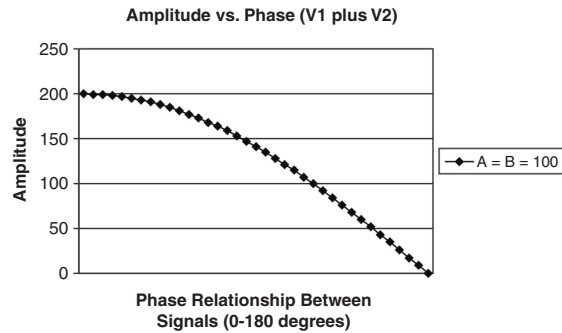
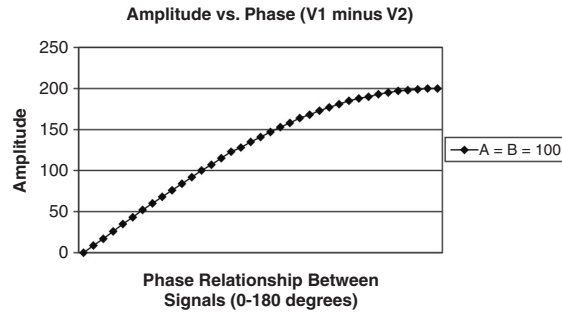


FIGURE 2. Amplitude-phase relationship of the difference between V_1 and V_2 when magnitudes are equal.

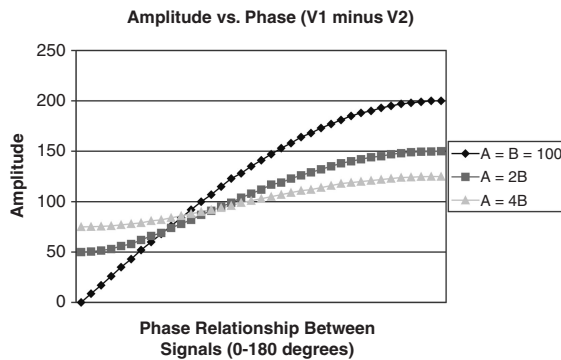


which one is effectively encouraging synchrony between the sites.

Conversely, when measuring the difference between vectors ($V_1 - V_2$), the resultant magnitude varies directly with increasing ϕ where the maximum magnitude is attained at $\phi = 180$ deg and the minimum at $\phi = 0$ deg, as shown in Figure 2. When performing bipolar training, we are concerned only with this relationship. Since the only difference between Figures 1 and 2 lies in the relative phase, it is apparent that bipolar placement serves effectively as a transducer of relative phase into net amplitude. It is, first and foremost, a phase discriminant.

The phase dependence is illustrated in Figure 3 for three assumptions of relative amplitudes of V_1 and V_2 . It is apparent that the phase dependence is most determinative in the event that A and B are of comparable amplitude. In cases where there is some amplitude disparity between generators, phase shifts will play a

FIGURE 3. Amplitude and phase for V1-V2 for three different amplitude ratios.



lesser but still significant role in resultant amplitudes. And finally, the case where B is much less than A can be taken to simulate the case of referential placement with ear reference. Relative phase still enters, but may no longer be predominantly determinative for the reward contingencies. (The case $B > A$ represents nothing new because the designations are arbitrary.)

In typical trainings, a threshold is selected such that a reward criterion is met for some percentage of the time (e.g., 70%). Whereas the respective amplitudes play into this, the probability of a reward is minimal unless a phase criterion is also met—hence the primacy of phase in training with bipolar placements. A sample Monte Carlo probability analysis illustrates this point for more realistic assumptions.

MONTE CARLO CALCULATION

In order to simulate the influence of phase on the net reward incidence in bipolar training, a Monte Carlo calculation was performed in which the respective amplitudes of V1 and V2, as well as their phase differences, were all allowed to vary randomly. The individual amplitudes were assumed to be Gaussian-distributed with amplitude ranging from 0 to 100. Phase was assumed to have a uniform distribution. There is no implication that phase is in fact randomly distributed, or that the amplitudes of V1 and V2 are in fact uncorrelated. Obviously such assumptions are violated in nature. It was simply of interest to examine the dependence of re-

ward incidence on relative phase. Results are shown in Figure 4 and indicate that large net signals tend to occur at large phase angles, as expected.

In customary usage a threshold is applied such that a reward issues nominally 70% of the time. Applying that criterion to the “data” of Figure 4 yields a threshold value of 42 on this scale. The resulting distribution of reward probability as a function of phase angle is given in Figure 5. A clear disfavoring of small phase angles is the most prominent feature. Some 97% of hits lie in range of 40 to 180 degrees in phase angle. Hence the training can be considered one that strongly disfavors phase synchrony.

The cumulative distribution derived from the incremental distribution in Figure 5 is shown in Figure 6. This figure illustrates that

FIGURE 4. Resultant distribution of amplitude values for randomized V1 and V2 magnitudes as a function of phase angle.

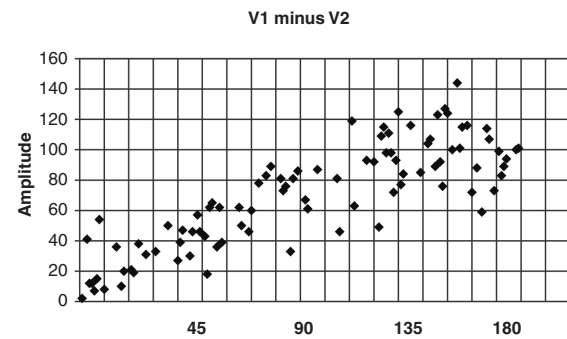


FIGURE 5. Percent of points above 70% threshold vs. phase.

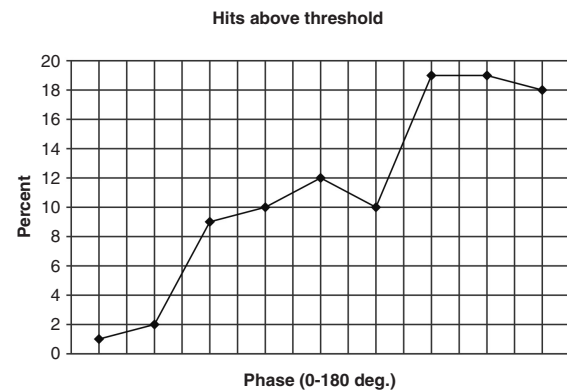
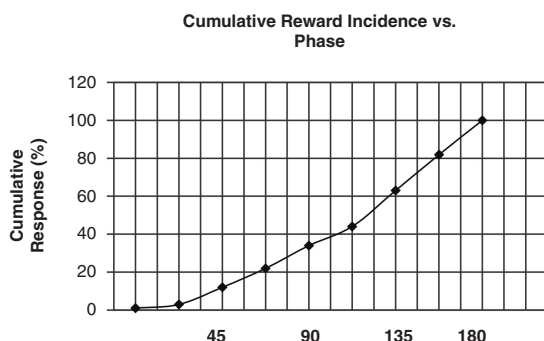


FIGURE 6. Cumulative reward incidence for 100 random trials, shown as a function of relative phase angle.



only three percent of rewards apply to the case of phase difference less than 40 degrees. With increasingly liberal reward criteria (which are often used), the requisite phase difference will decrease. Thus when performing bipolar training with generous thresholding, the range of phase over which success can be readily achieved is even broader. However, even with a liberal reward scheme we are still encouraging an “anywhere but here” response by the brain (i.e., any phase but synchrony).

Since inhibits in neurofeedback amount to nothing more than the withholding of a reward, one could equivalently see the reward-based training in terms of an inhibit on synchronous activity. More specifically, one can consider bipolar training in terms of a “soft inhibit” over a certain range in relative phase, in contrast to the “hard inhibits” we place on amplitudes. Equivalently, one can think of this in terms of an exclusion zone in terms of phase, in this one with soft rather than hard boundaries. This is best illustrated in Figure 7, where Figure 2 has been redrawn as a polar plot. The soft exclusion zone is to be found symmetrically distributed around zero phase angle. It will be observed that the phase dependence of the net signal is very strong within that zone, which motivates our perspective that phase is the driver in bipolar training of the kind being discussed here. Seen in this “inhibit-based” perspective, Figure 7 illustrates the large phase space available for rewards outside of the narrow exclusion zone.

DISCUSSION

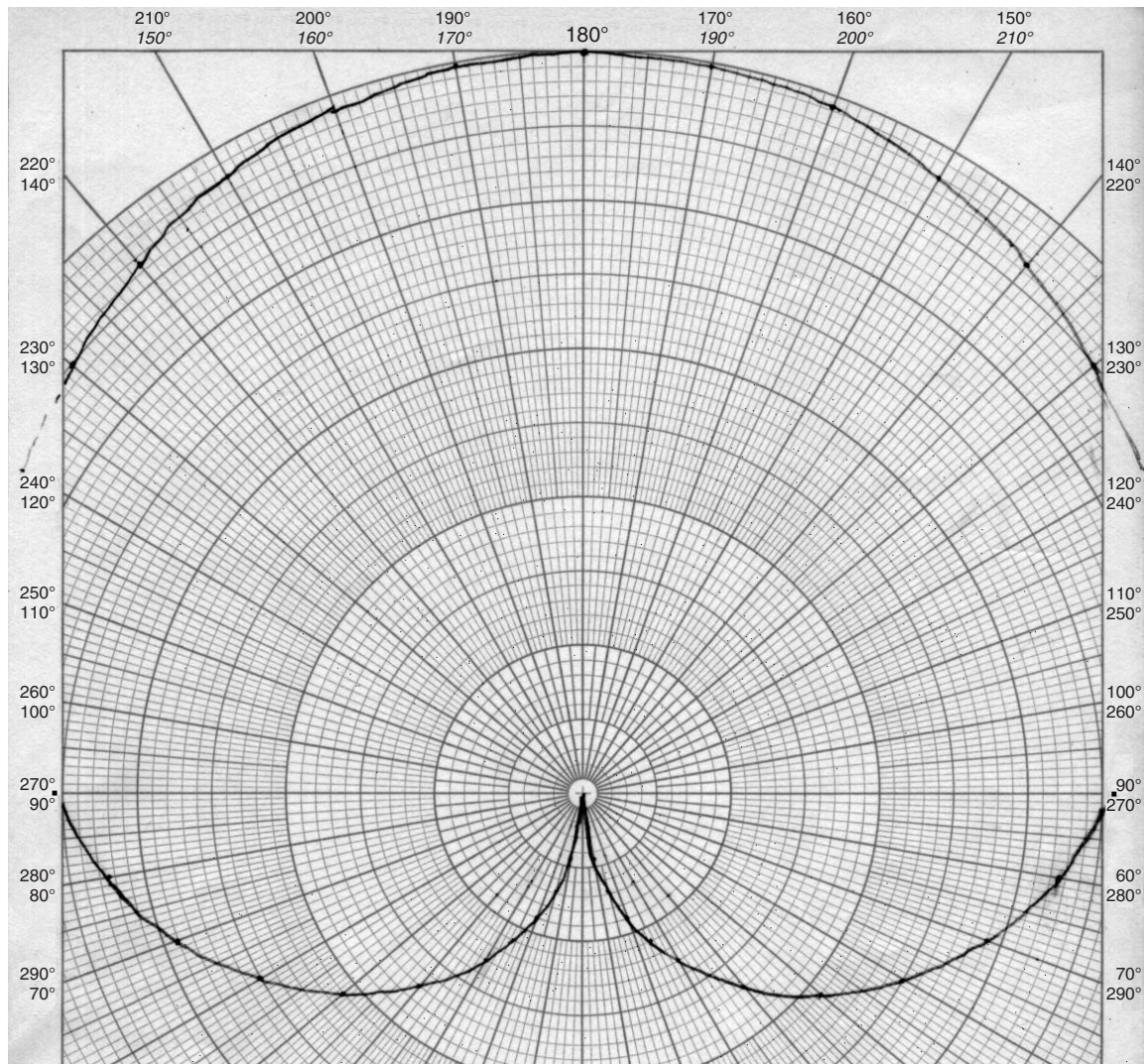
The principal motivation for this exercise was to make explicit the relationships that are relevant to inter-hemispheric training at homologous sites. The results of Figure 4 through Figure 7 support the view that the training implicitly rewards non-synchronous activity. This holds true even under the assumption of random amplitudes at the two sites. In reality of course, the amplitudes are somewhat correlated, and in that event the dominance of relative phase in the net reward incidence is even stronger, as illustrated in the top curve of Figure 3.

This treatment is equally applicable to near-neighbor sites, where elevated coherence is expected. Because amplitudes are somewhat correlated between near-neighbor sites, the impact of relative phase on reward incidence is likewise expected to be strong. Hence, bipolar training with near-neighbor placement can also be regarded in terms of promoting desynchronization, as opposed to viewing it in terms of the standard amplitude up-training. Note that the term “desynchronization” is used to describe a condition in which the phase angle is non-zero. This does not necessarily imply anything about coherence.

Finally, when excesses in EEG amplitudes are observed at certain frequencies, and reward training with bipolar placement is used in the same EEG band, the result will be a tendency toward desynchronization rather than an exacerbation of the amplitude deviation. In other words, fears about the arbitrary use of this protocol in the face of amplitude elevations are unfounded. Clinical experience is in accord with this conclusion (Othmer, 2005).

It is an implicit assumption of this work that training toward desynchronization of the EEG effectively trains down excess coherence. The apparent conflation of these two concepts (synchrony and coherence) is defensible on the basis of findings by Hudspeth that if the phase delay is greater than the equivalent of 10 milliseconds, coherence drops toward insignificance in any event (Hudspeth, 2000). Thus synchrony is in most instances of clinical import, and at most frequencies employed in EEG training, a viable stalking horse for coherence. At a minimum, the two measures co-vary. It is

FIGURE 7. Polar plot of net amplitude as a function of relative phase angle. This is simply a re-plotting of Figure 2 (V1-V2)



therefore quite defensible to refer to reward training with bipolar placement in terms of the down-training of coherence.

Coherence excesses represent an obvious and common failure mode of the regulation of cortical timing. However, such excesses do not characterize all of the conditions for which interhemispheric training has been found to be helpful. In such cases, one must necessarily think of this training simply as a challenge to the regulatory mechanisms by which interhemispheric timing is organized. Merely the deviation from prevailing states that is evoked through feedback provokes a reaction by the

brain in a restorative direction. The repetition of this push/pull dynamic eventuates ultimately in improved regulatory performance. Thus, the training may not have to be directed against a particular target of training at all. It may be sufficient simply to mildly challenge the brain out of its prevailing state. If that is the case, then the distinction between synchrony and coherence is once again a secondary consideration. If the challenge is non-prescriptive, then it also follows that the clinical benefits should be diagnostically non-specific (see Othmer, 2005).

In summary, the brain must organize timing between the hemispheres, and these dynamics

become evident through phase relationships. Bipolar placement serves as a transducer of relative phase into amplitude and thus makes phase accessible as a dynamic training variable. Interhemispheric training at homologous sites represents a challenge to the networks and the mechanisms that govern such timing. The training may serve to move the cortex out of the ambient state into a slightly different state. This, in turn, activates a restorative response by the brain that moves it back toward the original intended state. The repetition of this action-reaction dynamic may serve to strengthen the operative regulatory loops. From this perspective, EEG training can be seen as a very subtle challenge to the brain's regulatory networks that manage global timing relationships.

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